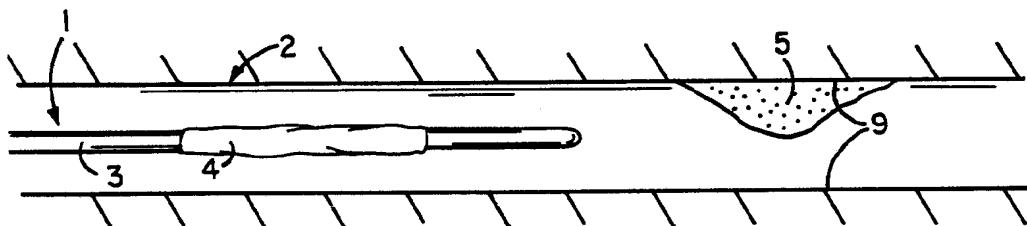




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## (54) Title: DRUG DELIVERY SYSTEM



## (57) Abstract

The invention features a catheter (1) and methods for delivering drug to tissue at a desired location of the wall of a body lumen (2). The catheter (1) is constructed for insertion in a body lumen (2) and has a catheter shaft (3) and an expandable portion (4) mounted on the catheter shaft (3). The expandable portion (4) is expandable to a controlled pressure to fill the cross-section of the body lumen (2) and press against the wall (9) of the body lumen (2). In one embodiment, at least a portion of the exterior surface of the expandable portion (4) is defined by a coating (6) of a tenaciously adhered swellable hydrogel polymer. Incorporated in the hydrogel polymer is an aqueous solution of a preselected drug (8) to be delivered to the tissue or plaque. The hydrogel polymer and drug (8) are selected to allow rapid release of a desired dosage of the drug (8) from the hydrogel polymer coating during compression of the hydrogel polymer coating against the wall (9) of the lumen (2) when the expandable portion (4) is expanded. In other embodiments the polymer is released from the expandable portion (4) in response to pressure, to coat the wall (9) of the body lumen (2).

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### DRUG DELIVERY SYSTEM

#### Field of the Invention

The invention relates to delivery of drugs to the  
5 walls of body lumens.

#### Background of the Invention

Systemic administration of drugs treats the organism as a whole, even though the disease may be localized, such as occlusion of a duct or vessel.

10 Localization of a drug poses special problems in cases involving the walls of ducts and vessels, since, by nature, these organs serve as transport systems.

Arthrosclerotic disease, for example, causes localized occlusion of the blood vessels resulting from  
15 the build-up of plaque. As the deposits increase in size, they reduce the diameter of the arteries and impede blood circulation. Angioplasty, which involves the insertion of catheters, such as balloon catheters, through the occluded region of the blood vessel in order  
20 to expand it, has been used to treat arthrosclerosis.

The aftermath of angioplasty in many cases is problematic, due to restenosis, or closing of the vessel, that can occur from causes including mechanical abrasion and the proliferation of smooth muscle cells stimulated  
25 by the angioplasty treatment. Restenosis may also occur as a result of clot formation following angioplasty, due to injury to the vessel wall which triggers the natural clot-forming reactions of the blood.

#### Summary of the Invention

30 In one aspect, the invention features a catheter and method for delivering drug to tissue at a desired location of the wall of a body lumen. The catheter is constructed for insertion in a body lumen and has a catheter shaft and an expandable portion mounted on the  
35 catheter shaft. The expandable portion is expandable to

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a controlled pressure to fill the cross-section of the body lumen and press against the wall of the body lumen. At least a portion of the exterior surface of the expandable portion is defined by a coating of a  
5 tenaciously adhered swellable hydrogel polymer. Incorporated in the hydrogel polymer is an aqueous solution of a preselected drug to be delivered to the tissue. The hydrogel polymer and drug are selected to allow rapid release of a desired dosage of the drug from  
10 the hydrogel polymer coating during compression of the hydrogel polymer coating against the wall of the lumen when the expandable portion is expanded.

Various embodiments may include one or more of the following features. The catheter is adapted for  
15 insertion in a blood vessel, and the expandable portion is an inflatable dilatation balloon adapted for inflation at pressures in the range for effecting widening of a stenosed blood vessel. The pressure is in the range of about 1 to 20 atmospheres. The hydrogel polymer and drug  
20 are effective to release about 20% or more of the drug during inflation in the pressure range. The compression is effective to deliver the drug over a duration of about 10 minutes or less. The hydrogel polymer coating is about 10 to 50 microns thick in the swelled, uncompressed  
25 state. The hydrogel polymer is selected from the group consisting of polycarboxylic acids, cellulosic polymers, gelatin, polyvinylpyrrolidone, maleic anhydride polymers, polyamides, polyvinyl alcohols, and polyethylene oxides. The hydrogel polymer is polyacrylic acid. The drug is an  
30 anti-thrombogenic drug selected from the group consisting of heparin, Pebac, enoxaprin, aspirin and hirudin. The drug is an anti-proliferative drug selected from the group consisting of monoclonal antibodies, capable of blocking smooth muscle cell proliferation, heparin,  
35 angiopeptin and enoxaprin. The expandable portion is

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adapted for application of heat to the polymer material to control the rate of administration. The catheter further comprises a sheath member, extendable over the balloon to inhibit release of the drug into body fluids  
5 during placement of the catheter. The balloon catheter is a perfusion catheter having an expandable balloon. The expandable portion includes a stent, mountable in the blood vessel by expansion thereof. The drug is bound in the hydrogel polymer for slow time release of the drug  
10 after the compression of the hydrogel polymer by the expansion. The hydrogel polymer is a polyacrylic acid including an ammonium anion and the drug is heparin. The stent is expandable by a balloon. The catheter where the stent and balloon both include the swellable hydrogel  
15 coating incorporating the drug. The expandable portion is prepared by introducing an aqueous solution of the drug to the hydrogel polymer coating, the catheter is introduced to the body lumen to position the expandable portion at the point of desired drug application, and the  
20 expandable portion is expanded to enable delivery of the drug by compression of the hydrogel polymer coating against the wall at the body lumen. The expandable portion is positioned at a point of occlusion in the blood vessel and expanding the expandable portion at  
25 pressures sufficient to simultaneously dilate the vessel and deliver the drug by compression of the hydrogel polymer coating.

In a particular aspect, the invention includes a balloon catheter for delivering drug to tissue at a  
30 desired location of the wall of a blood vessel. The catheter is constructed for insertion in a blood vessel and has a catheter shaft and an expandable dilatation balloon mounted on the catheter shaft. The expandable balloon is expandable by an expansion controller to  
35 engage the tissue at a controlled pressure in the range

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of about 1 to 20 atmospheres to fill the cross-section of the blood vessel and press against the wall of the blood vessel. At least a portion of the exterior surface of the expandable balloon is defined by a coating of a tenaciously adhered swellable hydrogel polymer with a thickness in the range of about 10 to 50 microns in the swelled state, and incorporated within the hydrogel polymer coating, an aqueous solution of a preselected drug to be delivered to the tissue. The hydrogel polymer and drug are selected to allow rapid release of a desired dosage of about 20% or more of the drug solution from the hydrogel polymer coating during compression of the hydrogel polymer coating against the wall of the vessel when the expandable portion is expanded in the pressure range.

In various embodiments, the hydrogel polymer is selected from the group consisting of polycarboxylic acids, cellulosic polymers, gelatin, polyvinylpyrrolidone, maleic anhydride polymers, polyamides, polyvinyl alcohols, and polyethylene oxides. The hydrogel polymer is polyacrylic acid. The drug is an anti-thrombogenic drug selected from the group consisting of heparin, Pebac, enoxaprin, aspirin and hirudin. The drug is an anti-proliferative drug selected from the group consisting of monoclonal antibodies, capable of blocking smooth muscle cell proliferation, heparin, angiopeptin and enoxaprin. The catheter further comprises a sheath member, extendable over the balloon to inhibit release of the drug into body fluids during placement of the catheter.

In another aspect, the invention features a catheter for delivering drug to tissue at a desired location of the wall of a body lumen, comprising. The catheter is constructed for insertion in a body lumen having a catheter shaft and an expandable portion mounted

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on the catheter shaft, the expandable portion is expandable to a controlled pressure to fill the cross-section of the body lumen and press against the wall of the body lumen. At least a portion of the exterior 5 surface of the expandable portion is defined by a coating of a body-fluid soluble polymer, and incorporated within the soluble polymer, a preselected drug to be delivered to the tissue. The soluble polymer and drug are selected to allow release of the polymer from the surface of the 10 balloon during compression of the polymer coating against the wall of the body lumen when the expandable portion is expanded to coat the wall of the body lumen.

Various embodiments include the following. The 15 polymer is selected from the group consisting of polycaprolactone, polyorthoesters, polylactic acids, polyglycolic acids, and albumin. The catheter where the drug is selected from anti-thrombogenic drugs and anti-proliferative drugs. The catheter where the expandable portion is adapted for application of heat to the polymer material to control the rate of administration. The 20 catheter where the polymer is a meltable polymer, and the release of the polymer is aided by the application of heat.

In general, an advantage of the invention is the 25 application of drugs by active diffusion directly into the tissue within the body requiring treatment. The drug is preferably applied in a rapid but low-stress, low energy manner that does not further injure the tissue to be treated, and administration is selectively and evenly 30 distributed over the treated area such that the drug can be taken up by tissue and plaque, without, e.g., being washed away by body fluids.

Description of Preferred Embodiments

We first briefly describe the drawings.

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Drawings

Figs. 1-1a are enlarged views of a method of preparing an embodiment of the invention.

Fig. 1b is an enlarged cross-sectional view of an embodiment of the drug delivery balloon catheter of the invention being moved through a vessel toward an occlusion to be treated.

Fig. 1c is an enlarged cross-sectional view of the balloon in Fig. 1b, now fully inflated and at the site of occlusion.

Fig. 1d is a further enlarged, schematic cross-sectional view of the portion of Fig. 1c indicated in the circle 1e, but taken prior to full inflation.

Fig. 1e, which corresponds to the portion of Fig. 1c indicated in the circle 1e, is an enlarged, schematic cross-sectional view, as in Fig. 1d, but with the balloon under full inflation to release the drug coated on the balloon.

Fig. 2 is an enlarged cross-sectional view of another embodiment of the drug delivery balloon catheter of the invention including a sheath for covering the catheter as it is being moved through a vessel toward the occlusion to be treated.

Fig. 2a is an enlarged cross-sectional view of the catheter of Fig. 2 with the sheath retracted and balloon inflated at the site of occlusion.

Fig. 3 is an enlarged, schematic cross-sectional view of another embodiment of the drug delivery balloon catheter in which the drug, originally held within a polymer applied to a thermal balloon of the invention, is now entering the surrounding tissue.

Fig. 3a is a further enlarged, schematic illustration of the embodiment of Fig. 3 and illustrates the entry of the drug, shown as circles, into the surrounding tissue.

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Figure 4 shows a balloon catheter with the hydrogel and drug coated endoprostheses mounted on the balloon section, in the region of the thrombus, before radial expansion of the balloon section and 5 endoprostheses.

Figure 4a is an enlargement of Figure 4 showing the hydrogel polymer and drug coated endoprostheses and Fig. 4b is a cross-section along the line b-b in Fig. 4a.

Figure 5 shows the endoprostheses compressed 10 against the vessel wall by radial expansion of the balloon section with the drug diffused into the compressed thrombus before removal of the balloon catheter.

Figure 6 shows the endoprostheses positioned 15 against the drug inside the compressed thrombus, after removal of the balloon catheter.

#### General Description

Referring to Figs. 1-1e, in one embodiment, the invention includes a drug delivery balloon catheter 20 device 1 comprising a catheter body 3 having a balloon 4 attached at its distal end. The balloon 4 on the catheter 3 includes a swellable hydrogel polymer coating 6. As shown in Figs. 1-1a, a drug 8 in an aqueous solution is absorbed into the hydrogel with the balloon 25 in the deflated state prior to insertion into the patient by the physician, e.g., the hydrogel-coated balloon may be immersed in a small tube or vial containing the drug. The drug may also be applied in the form of droplets, such as from an eyedropper, or the drug may be 30 precipitated into the hydrogel prior to sterilization and sold as a finished device. Exposure of the hydrogel to the solution causes the hydrogel to swell.

As shown in Fig. 1b, typically the device 1 is inserted into the duct or vessel 2 having a region to be 35 treated, such as an occlusion due to a deposition of

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plaque 5 on the vessel wall tissue 9. The device 1 is moved along the vessel to position the balloon 4 at the occlusion site, as shown in Fig. 1c. The vessel may be, for example, a narrow, tortuous opening through which the catheter is passed by torquing from the distal end. As the balloon is inflated the pressure created by the balloon against the tissue compresses the hydrogel and the drug is quickly and freely released for transfer by active diffusion into the plaque and tissue. The pressure applied to the plaque and tissue by the expansion of the balloon during application of the drug enhances transfer of the drug into the tissue and plaque. This process is referred to here as active diffusion. The balloon and catheter may be exposed to the body fluids of the lumen for a considerable time, e.g., up to about 15 minutes in some angioplasty procedures. An advantage of this invention is that large amounts of the drug, e.g., greater than 20%, even 30-50% or more, of the drug solution contained in the hydrogel, is diffused into the effected area in the short time duration which the hydrogel is compressed, e.g., 2-10 minutes after the balloon is inflated at the treatment site. The inflation pressure needed to dilate the vessel which also approximates the compression of the coating, is in the range of 1 to 20, typically about 2 to 10 atmospheres. The balloon is preferably a compliant material such as polyethylene which conforms to the shape of the lumen wall. The balloon may also be formed of other materials used in angioplasty, e.g., a nondistending material, such as polyethylene terephthalate (PET). Transporting the drug in the hydrogel prevents substantial release of the drug to body fluids prior to reaching the treatment area and during the drug application phase and allows large dosages to be delivered at a desired location.

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In the embodiment of Fig. 1c, the balloon coating 6 is a swellable, compressible coating formed of the hydrogel and drug in solution. In Fig. 1d, the balloon 4 is shown inflated such that the coating 6, which has an initial thickness, is in contact with the occlusion 5 but not under substantial pressure. Further inflation of the balloon 4, as shown in Fig. 1e, compresses the hydrogel coating 6 against the occluded areas 5 causing quick release of the drug (represented by circles) contained in the coating 6 directly into the plaque and nearby healthy tissue, as indicated by the directional arrows, much in the nature of squeezing liquid from a sponge. The introduction of the drug into the plaque and tissue occurs simultaneously with widening of the occlusion by the dilatation balloon. Thus, as cracking of the plaque and stimulation of smooth muscle cells beneath the plaque and along healthy tissue of the vessel wall are caused by dilatation, a therapeutic drug is simultaneously applied to the effected area, e.g., to counteract the effects of the trauma. The thickness of the balloon 4 remains substantially the same, while the thickness of the coating 6 decreases due to the compression of the coating and the release of the drug 8. (Figs. 1d-1e are schematic drawings and are not to scale with respect to the thickness of the balloon relative to the thickness of the hydrogel coating.) The drug carried by the balloon is evenly applied to plaque and tissue and isolated by the pressure of the balloon from the flow of body fluids in the lumen such that the drug, e.g., an anti-proliferative, may actively diffuse through the cracks formed in the plaque and reach the smooth muscle tissue. (It will also be understood that, as an alternative procedure, after dilation with a conventional angioplasty balloon catheter, a catheter carrying a drug-delivery,

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inflatable balloon, such as has been described, may be used to treat the vessel.)

The hydrogel coating is characterized by the ability to incorporate a substantial amount of the drug, typically in aqueous solution form, and is swellable such that the aqueous drug solution can be effectively squeezed out of the coating when pressure is applied by inflation of the balloon. Administration of the drug in this way enables the drug to be site specific, such that release of high concentrations and/or highly potent drugs may be limited to direct application to the diseased tissue. Furthermore, the drug is applied to the diseased tissue by the sponge-like coating in an even, gentle manner without disrupting or injuring the healthy tissue, while diffusion of the drug into the tissue is facilitated by the application of the pressure of the inflated balloon. The pressure also effectively forms a seal that prevents the flow of body fluids from washing the drug downstream of the treatment area. The dosage applied to the tissue may be controlled by regulating the time of presoaking the drug into the hydrogel coating to determine the amount of absorption of the drug solution by the hydrogel coating. Other factors affecting the dosage are the concentration of the drug in the solution applied to the coating and the releasability of the hydrogel coating, determined by, for example, the thickness of the hydrogel coating, its resiliency, porosity and the ability of the hydrogel coating to retain the drug, e.g., electrostatic binding or pore size, or the ionic strength of the coating, e.g., changed by changing the pH.

The drug may be an anti-thrombogenic drug, such as heparin or a heparin derivative, Pebac (dextrophenylalanine proline arginine chloromethylketone) or an anti-proliferative, such as heparin (also known to

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have anti-proliferative properties), enoxaprin, angiopeptin, or monoclonal antibodies capable of blocking smooth muscle cell proliferation, or it may be hirudin or acetylsalicylic acid (i.e., aspirin). Dosages applied to  
5 the tissue, for example, of heparin are typically in the range of 10-30 mg of heparin solution containing 200-1,000 units of sodium heparin. For use with hydrogels, the drug is preferably water soluble, so that the drug may be easily absorbed into the coating matrix.

10 The sponge-like characteristics of the hydrogel allows the aqueous drug solution to be effectively squeezed out of the coating when pressure is applied by inflation of the balloon. The hydrogel and drug combination are preferably noncomplexed, i.e., held  
15 together through the ability of the hydrogel to swell and absorb the drug solution, thereby allowing the preferable free-release of the drug at the treatment site.

20 In particular embodiments it may be advantageous to select a hydrogel coating for a particular drug such that the drug is not substantially released into body fluids prior to application of pressure by expansion of the balloon. Binding of the drug may also be accomplished by electrostatic attraction of the drug to the coating or a coating additive or by mechanical  
25 binding, e.g., employing a coating having a pore size that inhibits inward flow of body fluids or outward flow of the drug itself, that might tend to release the drug. Hydrogels are particularly advantageous in that the drug is held within the hydrogen-bond matrix formed by the  
30 gel.

35 The hydrogel is a cross-linked polymer material formed from the combination of a colloid and water. Cross-linking reduces solubility and produces a jelly-like polymer that is characterized by the ability to swell and absorb a substantial amount of the drug,

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typically in aqueous solution form. The hydrogel coating is also particularly hydrophilic, water swellable, and lubricous (i.e., having a low coefficient of friction). Preferred hydrogels are polyacrylic acid polymers 5 available as HYDROPLUS® (Boston Scientific, Watertown, MA) and as described in U.S. Patent application no. 297,331, filed January 17, 1991, the entire contents of which are hereby incorporated by reference). The drug, e.g., heparin in aqueous solution, is absorbed into the 10 coating without complexing and is freely released therefrom. Such hydrogel-drug combinations deliver about half of the drug solution in response to pressures in the range of balloon angioplasty in the vascular system. In other particular embodiments, the hydrogel polymer 15 includes acid groups and incorporates a drug which is anionic in nature that is bound by electrostatic attraction to cations in the coating, such as an ammonium cation, as described in "Lubricous Antithrombogenic Catheters, Guidewires, and Coatings," by Ronald Sahatjian 20 et al., USSN 7/451,507, filed on December 15, 1989, the entire contents of which are hereby incorporated by reference (see also corresponding International Publication No. WO91/08790, published June 27, 1991). The coating incorporating the quaternary ammonium salt is 25 effective to deliver an initial fast release of drug during compression and a slow release of drug remaining in the compressed coating after compression and is particularly useful for coating vascular stents as described further below.

30 In general, when dry, the hydrogel coating is preferably on the order of about 1 to 10 microns thick, with a 2 to 5 micron coating typical. Very thin hydrogel coatings, e.g., of about .2-.3 microns (dry) and much thicker hydrogel coatings, e.g., more than 10 microns 35 (dry), are also possible. Typically, the hydrogel

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coating thickness may swell by about a factor of 6 to 10 or more when the hydrogel coating is hydrated. For example, a hydrogel coating of about 1 to 3 microns thickness, when dry, usually swells to about 10-30  
5 microns thickness, when hydrated. Most preferably, the thickness of the coating is about 10 to 50 microns in the swelled, uncompressed state, and incorporates about 20-30mg of drug solution.

Referring to Fig. 2, in another embodiment of a  
10 drug delivery balloon catheter, the catheter 3 is preferably very small in diameter and flexible, much in the nature of a guidewire, formed, in this case, of hollow tubing to which the coated balloon 4 is attached. The balloon is covered by a protective sheath 7 while the instrument 1 is inserted into the vessel or duct 2 and positioned at the treatment region. As the coated  
15 balloon 4 is positioned at the occluded site 5, (Fig. 2a) the protective sheath 7 is drawn back to expose the balloon 4. In an alternative embodiment, the sheath  
20 remains stationary while the guidewire-like catheter moves the coated balloon forward into the occluded region. The sheath 7 protects the coating and inhibits premature release of the drug. Such a sheath might be particularly advantageous with coatings and drugs without substantial chemical or mechanical binding.  
25 Additionally, the balloon catheter may be a thermal balloon catheter with electrodes 43, as more fully described below. The application of such heat may be employed to facilitate the release of the drug from the coating, to facilitate penetration of the drug into the tissue, or to facilitate the therapeutic action of the drug.  
30

A procedure for preparing a drug delivery balloon with a hydrogel coating and an experiment of drug

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delivery for the above embodiments are presented in the following examples.

Examples

Example 1

5        A hydrogel coating on an angioplasty balloon may  
be formed as follows. The surface of the balloon  
(polyethylene) of an angiographic catheter is prepared by  
wiping down with clean cloth. The balloon has an O.D.  
(outer diameter) of about 3.5 mm (inflated). The balloon  
10      is coated with a solution of 4,4' diphenylmethane  
diisocyanate (MDI) in methylethylketone for 30 minutes.  
After drying in an air oven at 85° C for 30 minutes, the  
balloon is dipped in a 1.7% solution of poly(acrylic  
acid) homopolymer having a molecular weight of about  
15      3,000,000 in dimethylformamide (DMF) and tertiarybutyl  
alcohol. After drying at about 85° C for 30 minutes, a  
smooth coating is obtained. The balloon is oven dried  
for 8 hours at 50° C. One function of the drying steps  
is to remove solvent from the coating. The surface of  
20      the balloon becomes instantly lubricous upon exposure to  
water. The polyisocyanate solution is at a concentration  
of about .5 to 10% by weight. The polyacrylic acid is at  
a concentration of about .1 to 10% by weight. The  
poly(carboxylic acid) to polyisocyanate molar ratio is  
25      generally about 1:1. The formation of the hydrogel is  
further described in USSN 297,331, incorporated supra.

A solution of heparin salt may be applied to the  
coating. The solution is 10,000 units heparin sodium  
injection (Fisher Scientific, Pittsburgh, PA) USP Grade  
30      (1000 units/ml which is then added to 650cc distilled  
water) and may be applied by dipping for, e.g., about 1  
minute at room temperature. The heparin does not form a  
complex with the hydrogel solution and is freely released  
in response to compression of the polymer.

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After a catheter is prepared for use as discussed above, the catheter may be introduced into the patient using the Seldinger technique and expanded at a desired location to compress the hydrogel and deliver the heparin  
5 solution.

Example 2

Delivery of a drug from a hydrogel coating on a balloon was investigated in the following experiment. Tritium-labeled Pebac was absorbed into a 3.5 mm Slider®  
10 (balloon catheter from Boston Scientific Corporation) balloon coated with about a 40 micron thick (in the swelled state) coating as described in Example 1. The coating was dried and the radioactivity was counted. The balloon was then wetted with saline to swell the coating  
15 area. The balloon was inflated over a period of about one minute to about 4 atmospheres and held at this pressure for about 10 minutes in a thrombus created in an AV shunt from a baboon. The balloon was withdrawn and the amount of the drug in the thrombus was counted with a  
20 radiation counter. The experiment was performed with two different balloons using two different concentrations of Pebac, one balloon with 1-2 mg Pebac, and one balloon with 4mg Pebac. Both balloons delivered about 50% of the Pebac into the thrombus.  
25

Other Embodiments

Referring to Fig. 3, in another embodiment, the drug 44 is held within a polymer coating applied to the exterior of a thermal balloon, central wall portions 42 of which are shown in Fig. 3. The balloon is positioned  
30 in the lumen in the region to be treated and inflated such that the polymer coating is in contact with the tissue as shown in Figs. 3-3a. Heating of the balloon 42 melts the polymer and releases the drug 44 in a gentle, even, low-energy manner into the affected tissue.  
35 Suitable polymers include, but are not limited to,

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albumin, and collagen, e.g., gelatin, such as gel foams, which typically melt between about 40-60° C or polyvinylpyrrolidone (PVP), which dissolves rapidly when heated. The thermal balloon typically operates between 5 40-80° C. A suitable heated balloon system for this embodiment or that of Fig. 2a is discussed in Lennox et al., "Heated Balloon Catheters and the Like," U.S. Patent No. 4,955,377, hereby incorporated by reference. Inflating liquid is heated as a result of  $I^2R$  losses by 10 radiofrequency current flowing in the inflation fluid, e.g., saline, between the electrodes 43 (see Figs. 2a and 3), the liquid in turn heating the balloon wall. In the alternative, drugs which melt and which could be applied either with a meltable or non-meltable polymer binder 15 might be used.

An advantage to the meltable coatings is that the polymer may be cross-linked, (e.g., by physical or chemical cross-linking) after application of the drug 44 to the balloon to inhibit release of the drug 44 as the 20 balloon 42 is introduced through the body lumen to the area of treatment. The polymer itself typically does not melt off the balloon, but rather softens in a manner permitting release. However, in embodiments where the polymer is bioabsorbable, e.g., polycaprolactone, 25 polyorthoesters, polylactic acids, and polyglycolic acids, some or even all of the polymer may dissolve off of the balloon.

The balloon may also be coated with a polymer incorporating a drug and inflated to press against the 30 wall of the body lumen, where the polymer is selected to separate from the balloon and coat the wall of the lumen, in response to such pressure with or without the application of heat from the balloon. After application of the polymer, the balloon can be deflated and removed. 35 In this embodiment, the polymer may be a blood soluble

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polymer such as albumin, collagen or the like, incorporating a drug such as heparin. The polymer produces a smooth coating on the wall of the lumen and releases the drug to the tissue over time as the polymer 5 dissolves. Other soluble polymers are meltable and bioabsorbable polymers discussed above.

In another embodiment (see Figures 4-6) an endoprostheses (stent) is used in combination with a balloon catheter drug delivery system. An endoprostheses 10 50 is placed over the balloon catheter 51, and then coated with a noncomplexed hydrogel coating 52. The drug 8, shown as circles, in aqueous solution is then absorbed into the hydrogel coating 52. The balloon 51 and hydrogel and drug coated endoprostheses 50 are slid until 15 they reach the region of the occlusion 53 in the vessel 54. This is shown in Fig. 4. An enlargement of the drug and hydrogel polymer coated endoprostheses 50 is shown in Figs. 4a and 4b (thickness of coating 52 is greatly exaggerated). After the balloon 51 and hydrogel and drug 20 coated endoprostheses 50 have been positioned inside the vessel 54, the endoprostheses 50 is radially expanded by the admission of pressure to the balloon 51 and compressed against the vessel wall 54 with the result that occlusion 53 is compressed, and the vessel wall 54 25 surrounding it undergoes a radial expansion. The pressure from inflating the balloon squeezes the hydrogel 52, freely releasing the drug 8 into the tissue. The endoprostheses 50 is held in position in the expanded state as shown in Fig. 5. The pressure is then released 30 from the balloon and the catheter is withdrawn from the vessel. Figure 6 shows the drug 8 inside the compressed thrombus with the endoprostheses expanded and left in position, with the balloon catheter being withdrawn from the lumen. It will be understood that only the 35 endoprostheses may include the hydrogel polymer coating.

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In the embodiments employing a hydrogel-coated stent, the hydrogel and drug are selected such that an initial high dosage of drug is delivered to adjacent tissue upon initial compression of the polymer and thereafter a slow, sustained time-release of drug remaining in the hydrogel polymer occurs. Preferred hydrogel-drug combinations are those that employ a binding of the drug, such as electrostatic binding, e.g., by using a polyacrylic acid hydrogel in combination with an ammonium cation and heparin. In this case, the coating continues to release drug after expansion of the stent and removal of the balloon catheter. The stent may be a balloon-expansible stent as described above or a self-expanding stent, e.g., of the type formed with superelastic materials such as Nitinol.

Any of the embodiments discussed herein can be used with a protective sheath as described in Figs. 2-2a. In addition, a heated balloon catheter may be used in all combinations of the embodiments above to enhance and control the rate of drug-solution delivery into tissue. Other compressible sponge-like polymers, e.g., non hydrogels which release drug solutions in response to pressure, might be used as described with respect to the embodiment of Fig. 1 et seq.

Still other embodiments are within the claims.

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Claims

1        1. A catheter for delivering drug to tissue at a  
2 desired location of the wall of a body lumen, comprising:

3              a catheter constructed for insertion in a body  
4 lumen having a catheter shaft and an expandable portion  
5 mounted on said catheter shaft, said expandable portion  
6 being expandable to a controlled pressure to fill the  
7 cross-section of the body lumen and press against the  
8 wall of said body lumen,

9              at least a portion of the exterior surface of the  
10 expandable portion being defined by a coating of a  
11 tenaciously adhered swellable hydrogel polymer, and  
12 incorporated within said hydrogel polymer, an aqueous  
13 solution of a preselected drug to be delivered to said  
14 tissue,

15              said hydrogel polymer and drug selected to allow  
16 rapid release of a desired dosage of said drug from said  
17 hydrogel polymer coating during compression of said  
18 hydrogel polymer coating against the wall of the lumen  
19 when said expandable portion is expanded.

1        2. The catheter of claim 1 wherein said catheter  
2 is a dilatation catheter adapted for insertion in a blood  
3 vessel, and said expandable portion is an inflatable  
4 dilatation balloon adapted for inflation at pressures in  
5 the range for effecting widening of a stenosed blood  
6 vessel.

1        3. The catheter of claim 2 wherein said pressure  
2 is in the pressure range of about 1 to 20 atmospheres.

1        4. The catheter of claim 1 or 2 wherein said  
2 hydrogel polymer and drug are effective to release about

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3    20% or more of said drug during inflation in said  
4    pressure range.

1                5. The catheter of claim 1 or 2 wherein said  
2    compression is effective to deliver said drug over a  
3    duration of about 10 minutes or less.

1                6. The catheter of claim 1 or 2 wherein said  
2    hydrogel polymer coating is about 10 to 50 microns thick  
3    in the swelled, uncompressed state.

1                7. The catheter of claims 1 or 2 wherein said  
2    hydrogel polymer is selected from the group consisting of  
3    polycarboxylic acids, cellulosic polymers, gelatin,  
4    polyvinylpyrrolidone, maleic anhydride polymers,  
5    polyamides, polyvinyl alcohols, and polyethylene oxides.

1                8. The catheter of claim 7 wherein said hydrogel  
2    polymer is polyacrylic acid.

1                9. The catheter of claim 1 or 2 wherein said drug  
2    is an anti-thrombogenic drug selected from the group  
3    consisting of heparin, Pebac, enoxaprin, aspirin and  
4    hirudin.

1                10. The catheter of claim 1 or 2 wherein said  
2    drug is an anti-proliferative drug selected from the  
3    group consisting of monoclonal antibodies, capable of  
4    blocking smooth muscle cell proliferation, heparin,  
5    angiopeptin and enoxaprin.

1                11. The catheter of claim 1 or 2 wherein said  
2    expandable portion is adapted for application of heat to  
3    said polymer material to control the rate of  
4    administration.

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1           12. The catheter of claim 1 or 2 wherein said  
2 catheter further comprises a sheath member, extendable  
3 over said balloon to inhibit release of said drug into  
4 body fluids during placement of said catheter.

1           13. The catheter of claim 2 wherein said balloon  
2 catheter is a perfusion catheter having an expandable  
3 balloon.

1           14. The catheter of any one of claims 1 or 2  
2 wherein said expandable portion includes a stent,  
3 mountable in said blood vessel by expansion thereof.

1           15. The catheter of claim 14 where said drug is  
2 bound in said hydrogel polymer for slow time release of  
3 said drug after said compression of said hydrogel polymer  
4 by said expansion.

1           16. The catheter from claim 15 where said  
2 hydrogel polymer is a polyacrylic acid including an  
3 ammonium anion and said drug is heparin.

1           17. The catheter of claim 14 wherein said stent  
2 is expandable by a balloon.

1           18. The catheter of claim 17 wherein said stent  
2 and balloon both include said swellable hydrogel coating  
3 incorporating said drug.

1           19. A balloon catheter for delivering drug to  
2 tissue at a desired location of the wall of a blood  
3 vessel, comprising:

4           a catheter constructed for insertion in a blood  
5 vessel having a catheter shaft and an expandable

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6 dilatation balloon mounted on said catheter shaft, said  
7 expandable balloon being expandable by an expansion  
8 controller to engage said tissue at a controlled pressure  
9 in the range of about 1 to 20 atmospheres to fill the  
10 cross-section of the blood vessel and press against the  
11 wall of said blood vessel,

12 at least a portion of the exterior surface of the  
13 expandable balloon being defined by a coating of a  
14 tenaciously adhered swellable hydrogel polymer having a  
15 thickness in the range of about 10 to 50 microns in the  
16 swelled state, and incorporated within said hydrogel  
17 polymer coating, an aqueous solution of a preselected  
18 drug to be delivered to said tissue,

19 said hydrogel polymer and drug selected to allow  
20 rapid release of a desired dosage of about 20% or more of  
21 said drug solution from said hydrogel polymer coating  
22 during compression of said hydrogel polymer coating  
23 against the wall of the vessel when said expandable  
24 portion is expanded in said pressure range.

1 20. The catheter of claim 19 wherein said  
2 hydrogel polymer is selected from the group consisting of  
3 polycarboxylic acids, cellulosic polymers, gelatin,  
4 polyvinylpyrrolidone, maleic anhydride polymers,  
5 polyamides, polyvinyl alcohols, and polyethylene oxides.

1 21. The catheter of claim 19 wherein said  
2 hydrogel polymer is polyacrylic acid.

1 22. The catheter of claim 17 or 19 wherein said  
2 drug is an anti-thrombogenic drug selected from the group  
3 consisting of heparin, Pebac, enoxaprin, aspirin and  
4 hirudin.

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1               23. The catheter of claim 17 or 19 wherein said  
2 drug is an anti-proliferative drug selected from the  
3 group consisting of monoclonal antibodies, capable of  
4 blocking smooth muscle cell proliferation, heparin,  
5 angiopeptin and enoxaprin.

1               24. The catheter of claim 19 wherein said  
2 catheter further comprises a sheath member, extendable  
3 over said balloon to inhibit release of said drug into  
4 body fluids during placement of said catheter.

1               25. A method for delivering drug to the tissue at  
2 a desired location of the wall of a body lumen,  
3 comprising:

4               providing a catheter constructed for insertion in  
5 a body lumen having a catheter shaft and an expandable  
6 portion mounted on said catheter shaft, said expandable  
7 portion being expandable to engage said tissue at a  
8 controlled pressure to fill the cross-section of the body  
9 lumen and press against the wall of said body lumen, at  
10 least a portion of the exterior surface of the expandable  
11 portion being defined by a coating of a tenaciously  
12 adhered swellable hydrogel polymer, by

13               selecting said hydrogel polymer coating and drug  
14 to allow rapid release of a desired dosage of said drug  
15 from said hydrogel polymer coating during compression of  
16 said hydrogel coating polymer against the wall of the  
17 vessel when said expandable portion is expanded,

18               preparing said expandable portion by introducing  
19 an aqueous solution of said drug to said hydrogel polymer  
20 coating,

21               introducing said catheter to said body lumen to  
22 position said expandable portion at the point of desired  
23 drug application, and

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24               expanding said expandable portion to enable  
25    delivery of said drug by compression of said hydrogel  
26    polymer coating against the wall at said body lumen.

1                 26. The method of claim 25 further comprising  
2    introducing said catheter to a blood vessel.

1                 27. The method of claim 26 further comprising  
2    positioning said expandable portion at a point of  
3    occlusion in said blood vessel and expanding said  
4    expandable portion at pressures sufficient to  
5    simultaneously dilate said vessel and deliver said drug  
6    by compression of said hydrogel polymer coating.

1                 28. The method of claim 27 wherein said  
2    expandable portion is a dilatation balloon expandable to  
3    pressures in the range of about 1 to 20 atmospheres.

1                 29. The method of claim 28 further comprising  
2    delivering about 20% or more of said drug solution during  
3    said compression.

1                 30. The method of claim 29 wherein said drug is  
2    delivered in about ten minutes or less.

1                 31. The method of claim 30 wherein said hydrogel  
2    polymer is selected from the group consisting of  
3    polycarboxylic acids, cellulosic polymers, gelatin  
4    polyvinylpyrrolidone, maleic anhydride polymers,  
5    polyamides, polyvinyl alcohols, and polyethylene oxides.

1                 32. The method of claim 31 wherein said hydrogel  
2    polymer is polyacrylic acid.

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1           33. The method of any one of claims 25, 26, or 32  
2 wherein said drug is an anti-thrombogenic drug selected  
3 from the group consisting of heparin, Pebac enoxaprin,  
4 aspirin and hirudin.

1           34. The method of any one of claims 25, 26, or 32  
2 wherein said drug is an anti-proliferative drug selected  
3 from the group consisting of monoclonal antibodies,  
4 capable of blocking smooth muscle cell proliferation,  
5 heparin, and enoxaprin.

1           35. The method of claim 25 or 26 wherein said  
2 expandable portion is adapted for application of heat to  
3 said polymer material to control the rate of  
4 administration.

1           36. The method of claim 25 or 26 wherein said  
2 expandable portion includes a stent, mountable in said  
3 body lumen by expansion thereof.

1           37. The method of claim 36 further comprising  
2 selecting a drug polymer wherein there is binding of said  
3 drug in said hydrogel polymer for slow time release of  
4 said drug after compression of said hydrogel polymer by  
5 said expansion.

1           38. The method of claim 36 wherein said stent is  
2 expandable by a balloon.

1           39. The method of claim 38 wherein said stent and  
2 balloon both include said swellable hydrogel polymer  
3 coating incorporating said drug.

1           40. A catheter for delivering drug to tissue at a  
2 desired location of the wall of a body lumen, comprising:

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3           a catheter constructed for insertion in a body  
4   lumen having a catheter shaft and an expandable portion  
5   mounted on said catheter shaft, said expandable portion  
6   being expandable to a controlled pressure to fill the  
7   cross-section of the body lumen and press against the  
8   wall of said body lumen,

9           at least a portion of the exterior surface of the  
10   expandable portion being defined by a coating of a body-  
11   fluid soluble polymer, and incorporated within said  
12   soluble polymer, a preselected drug to be delivered to  
13   said tissue,

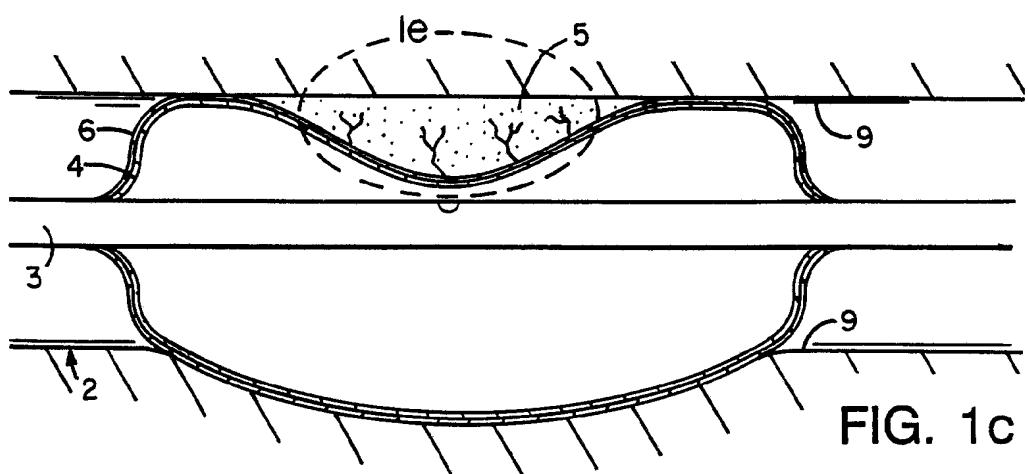
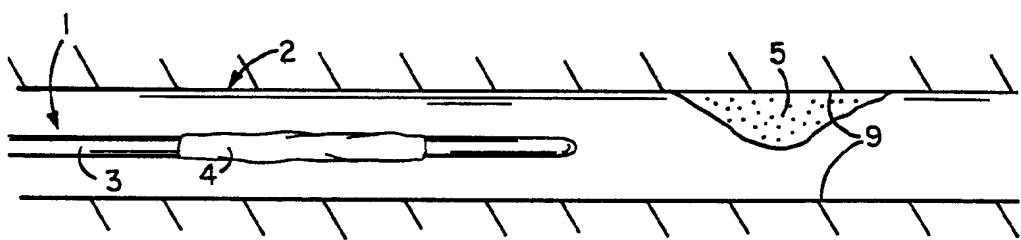
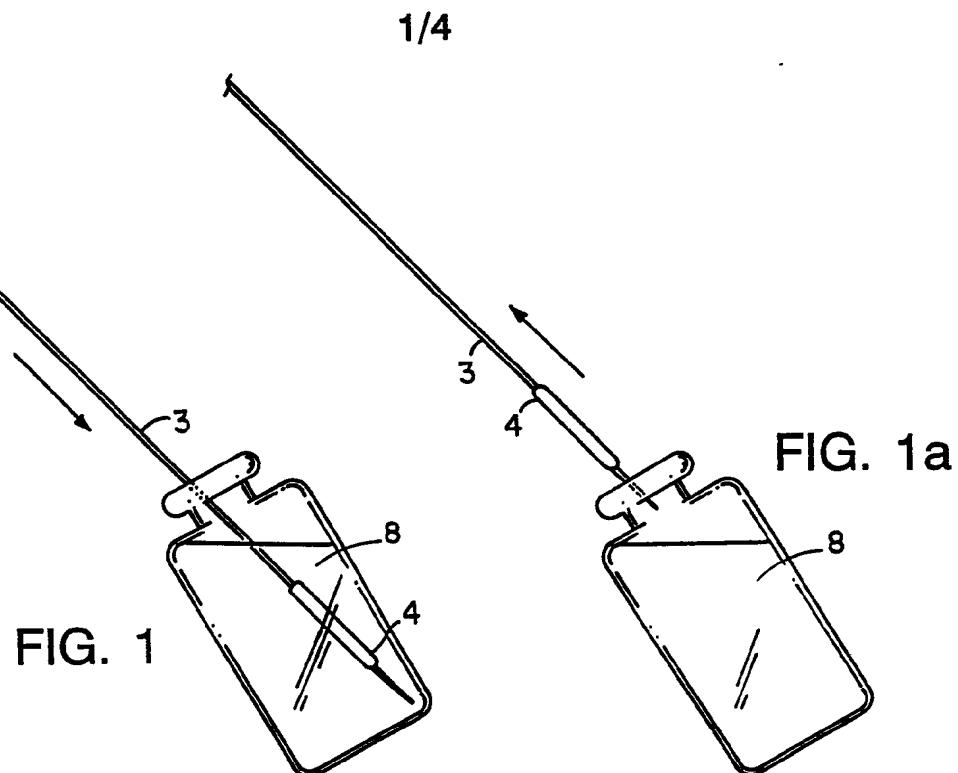
14           said soluble polymer and drug selected to allow  
15   release of said polymer from the surface of said balloon  
16   during compression of said polymer coating against the  
17   wall of said body lumen when said expandable portion is  
18   expanded to coat the wall of said body lumen.

1           41. The catheter of claim 40 where said polymer  
2   is selected from the group consisting of  
3   polycaprolactone, polyorthoesters, polylactic acids,  
4   polyglycolic acids, and albumin.

1           42. The catheter of claim 40 where said drug is  
2   selected from anti-thrombogenic drugs and anti-  
3   proliferative drugs.

1           43. The catheter of claim 40 wherein said  
2   expandable portion is adapted for application of heat to  
3   said polymer material to control the rate of  
4   administration.

1           2           44. The catheter of claim 43 where said polymer  
3   is a meltable polymer, and said release of said polymer  
4   is aided by the application of heat.



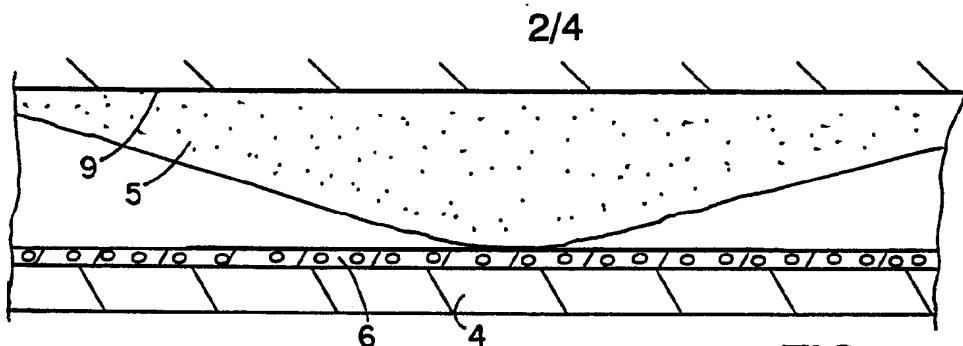


FIG. 1d

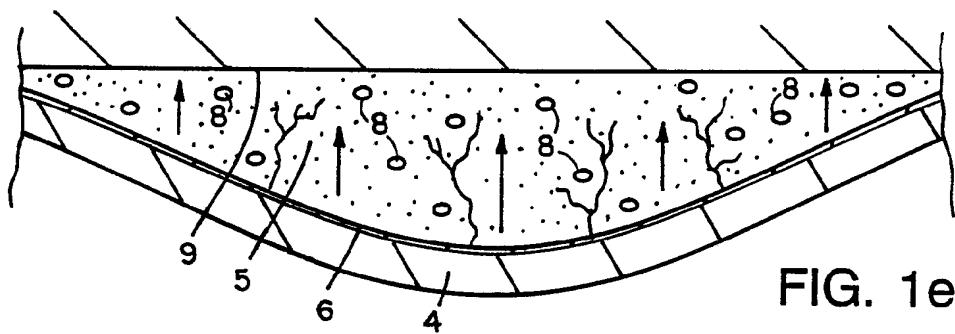


FIG. 1e

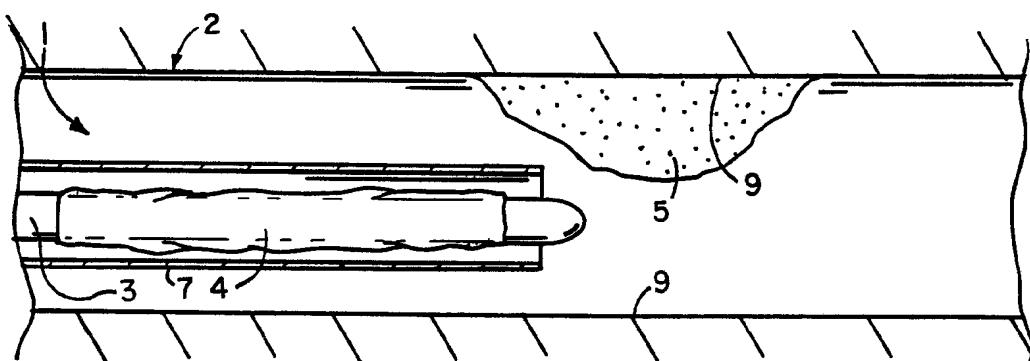


FIG. 2

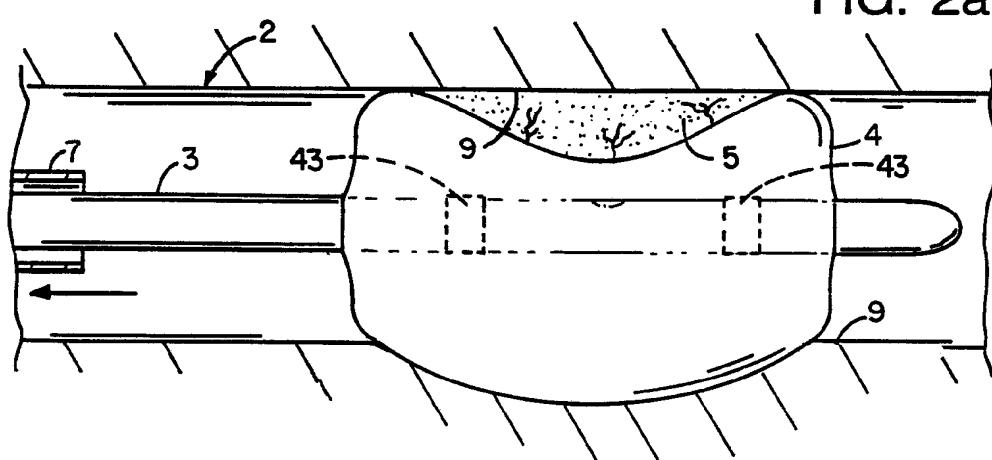


FIG. 2a

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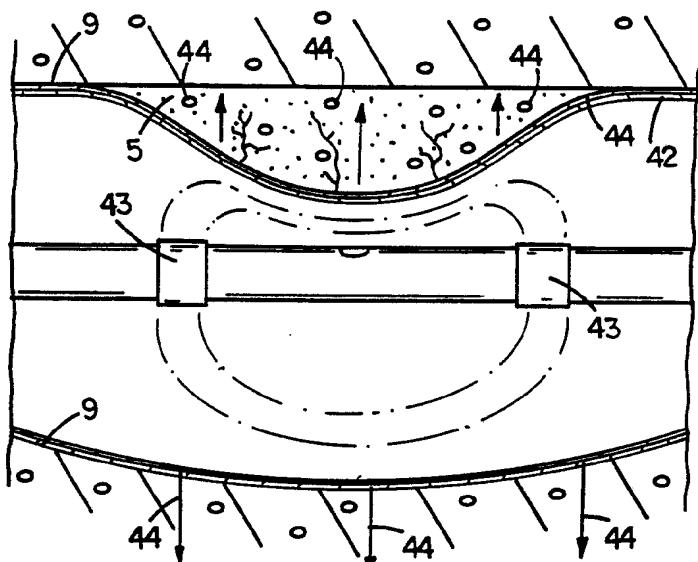


FIG. 3

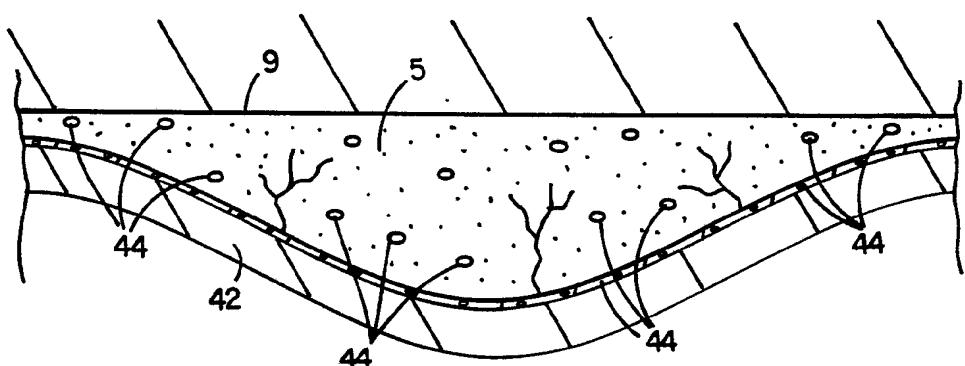


FIG. 3a

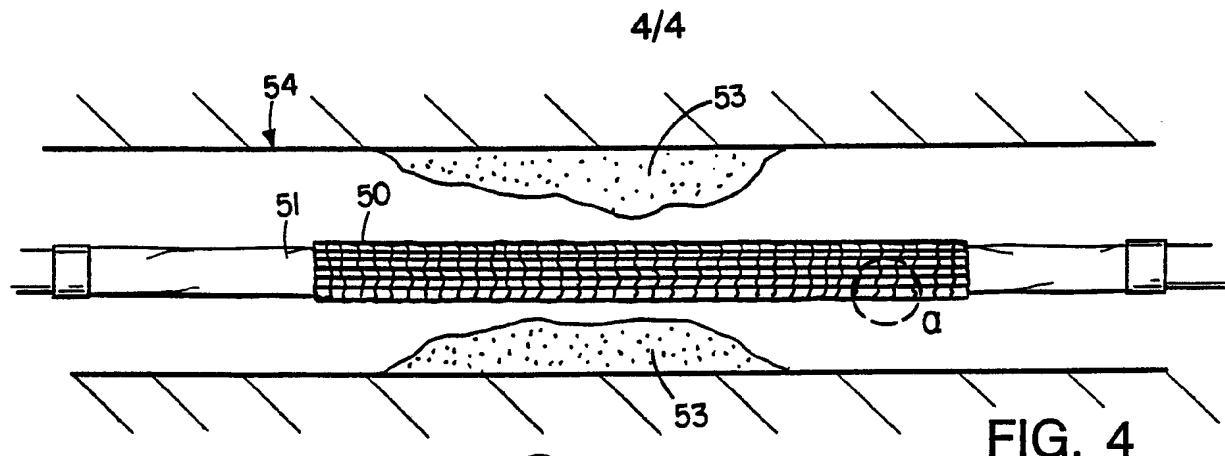


FIG. 4

FIG. 4a

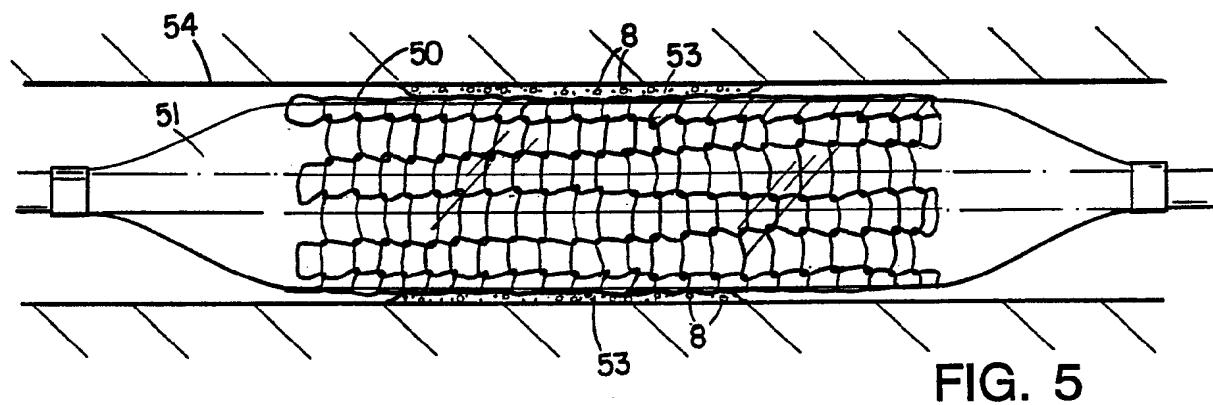
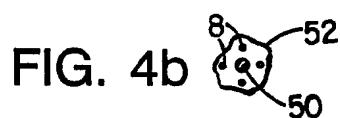
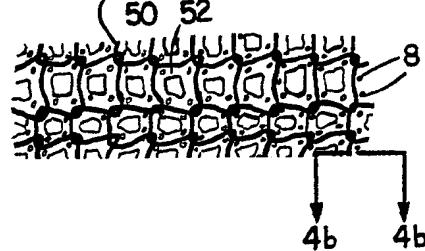


FIG. 5

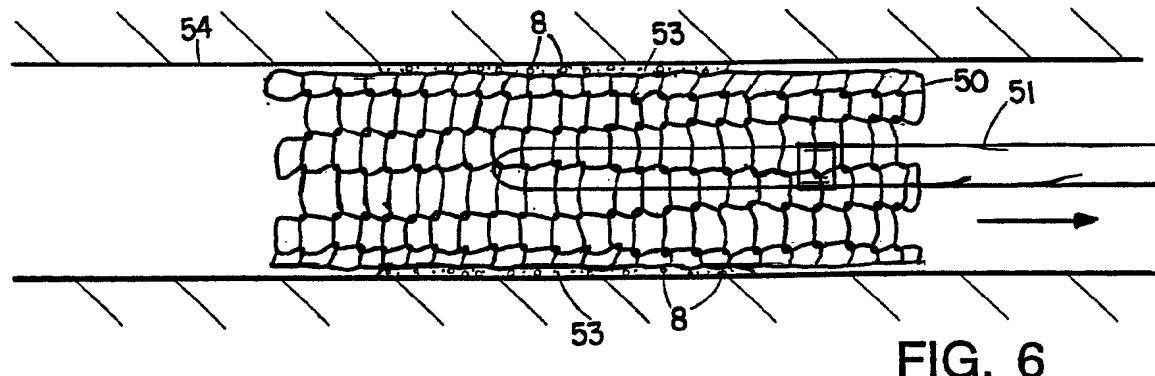


FIG. 6

# INTERNATIONAL SEARCH REPORT

International Application No. PCT/US91/09805

## I. CLASSIFICATION OF SUBJECT MATTER (if several classification symbols apply, indicate all) \*

According to International Patent Classification (IPC) or to both National Classification and IPC  
 IPC(5): A61M 31/00; A61M 29/00; A61M 5/32  
 U.S. CL.: 604/53,96,265

## II. FIELDS SEARCHED

Minimum Documentation Searched ?

Classification System	Classification Symbols
U.S.	604/53,96,99,101,265,266,890.1,892.1 606/192,194

Documentation Searched other than Minimum Documentation  
to the Extent that such Documents are Included in the Fields Searched \*

## III. DOCUMENTS CONSIDERED TO BE RELEVANT \*

Category *	Citation of Document, <sup>11</sup> with indication, where appropriate, of the relevant passages <sup>12</sup>	Relevant to Claim No. <sup>13</sup>
A	US,A, 4,515,593 (NORTON) 07 MAY 1985 See column 3 line 59 to column 5 line 35	1-44
A	US,A, 4,769,013 (LORENZ et al.) 06 SEPTEMBER 1988 See column 2 lines 8-64, column 4 lines 39-58	1-44
X Y	US,A, 4,950,256 (LUTHER et al.) 21 AUGUST 1990 See column 3 line 60 to column 4 line 23. See column 4 line 34-39. See column 5 line 6 to column 6 line 45. See column 9 line 1 to column 10 line 15. See column 10 lines 54-68	1,2,9,10,13,15 25-27,33,34  3-8,16,19-23, 28-32,40-42
A,P	US,A, 5,026,607 (KIEZULAS) 25 JUNE 1991 See column 1 line 40 to column 2 line 7. See column 3 line 7 to column 4 line 13	1-44
Y,P A,P	US,A, 5,041,100 (ROWLAND et al.) 20 AUGUST 1991 See column 1 line 59, to column 4 line 31.	1-10,13,16,19- 23,25-34,40-42  11,12,14,17,18 24,35-39,43,44

\* Special categories of cited documents: <sup>10</sup>

- "A" document defining the general state of the art which is not considered to be of particular relevance
- "E" earlier document but published on or after the international filing date
- "L" document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified)
- "O" document referring to an oral disclosure, use, exhibition or other means
- "P" document published prior to the international filing date but later than the priority date claimed

"T" later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention

"X" document of particular relevance; the claimed invention cannot be considered novel or cannot be considered "obvious".

"Y" document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art.

"&" document member of the same patent family

## IV. CERTIFICATION

Date of the Actual Completion of the International Search

11 FEBRUARY 1992

Date of Mailing of the International Search Report

08 APR 1992

International Searching Authority

ISA/US

Signature of Authorized Officer: SHARON E. FINKEL  
INTERNATIONAL DIVISION  
In: SHARON E. FINKEL *Sharon E. Finkel*